

New directions in EEG measurement: an investigation into the fidelity of electrical potential sensor signals

Article (Published Version)

Fatoorechi, M, Schwartzman, D, Prance, H, Parkinson, J, Seth, A K and Prance, R J (2015) New directions in EEG measurement: an investigation into the fidelity of electrical potential sensor signals. *Sensors & Transducers*, 184 (1). pp. 101-107. ISSN 2306-8515

This version is available from Sussex Research Online: <http://sro.sussex.ac.uk/53828/>

This document is made available in accordance with publisher policies and may differ from the published version or from the version of record. If you wish to cite this item you are advised to consult the publisher's version. Please see the URL above for details on accessing the published version.

Copyright and reuse:

Sussex Research Online is a digital repository of the research output of the University.

Copyright and all moral rights to the version of the paper presented here belong to the individual author(s) and/or other copyright owners. To the extent reasonable and practicable, the material made available in SRO has been checked for eligibility before being made available.

Copies of full text items generally can be reproduced, displayed or performed and given to third parties in any format or medium for personal research or study, educational, or not-for-profit purposes without prior permission or charge, provided that the authors, title and full bibliographic details are credited, a hyperlink and/or URL is given for the original metadata page and the content is not changed in any way.

New Directions in EEG Measurement: an Investigation into the Fidelity of Electrical Potential Sensor Signals

¹ M. FATOORECHI, ^{2,3} D. SCHWARTZMAN, ¹ H. PRANCE,
^{2,4} J. PARKINSON, ^{2,3} A. K. SETH, ¹ R. J. PRANCE

¹ Department of Engineering and Design, University of Sussex, Brighton, BN1 9QT, UK

² Sackler Centre for Consciousness Science, University of Sussex, Brighton, BN1 9QT, UK

³ Department of Informatics, University of Sussex, Brighton, BN1 9QT, UK

⁴ School of Psychology, University of Sussex, Brighton, BN1 9QT, UK

¹ Tel.: +441273872643, fax: +441273 877873

E-mail: M.Fatoorechi@sussex.ac.uk

Received: 14 November 2014 / Accepted: 15 December 2014 / Published: 31 January 2015

Abstract: Low frequency noise performance is the key indicator in determining the signal to noise ratio of a capacitively coupled sensor when used to acquire electroencephalogram signals. For this reason, a prototype Electric Potential Sensor device based on an auto-zero operational amplifier has been developed and evaluated. The absence of 1/f noise in these devices makes them ideal for use with signal frequencies ~10 Hz or less. The active electrodes are designed to be physically and electrically robust and chemically and biochemically inert. They are electrically insulated (anodized) and have diameters of 12 mm or 18 mm. In both cases, the sensors are housed in inert stainless steel machined housings with the electronics fabricated in surface mount components on a printed circuit board compatible with epoxy potting compounds. Potted sensors are designed to be immersed in alcohol for sterilization purposes. A comparative study was conducted with a commercial wet gel electrode system. These studies comprised measurements of both free running electroencephalogram and Event Related Potentials. Quality of the recorded electroencephalogram was assessed using three methods of inspection of raw signal, comparing signal to noise ratios, and Event Related Potentials noise analysis. A strictly comparable signal to noise ratio was observed and the overall conclusion from these comparative studies is that the noise performance of the new sensor is appropriate. *Copyright © 2015 IFSA Publishing, S. L.*

Keywords: Sensors, EEG, Biosensors, Assistive technology, Electrical Potential Sensor.

1. Introduction

The traditional methods employed for the acquisition of electroencephalogram (EEG) signals rely on the use of wet silver/silver chloride (Ag/AgCl) transducing electrodes. These convert ionic current on the surface of the body to electronic current for amplification and subsequent signal processing. Such electrodes are cheap and disposable

but require the use of a conducting gel between the electrode and the skin, since they rely on maintaining a low electrical resistance contact [1]. Operationally significant care is required in the preparation of the skin, usually involving abrasion, by skilled personnel. In addition, the gel may cause skin irritation and discomfort as well as drying out after a period of time, meaning that wet electrodes are unsuited to long term monitoring applications [2]. The gel may

also be responsible for cross coupling or shorting between electrodes in an array if great care is not taken during placement. Dry conducting electrodes provide a more user-friendly approach with electrodes making only resistive contact with the skin [3]. This overcomes the problems caused by the wet electrode gel, but introduces an additional variable, namely the variation in contact resistance due to perspiration, skin creams, or other individual differences in physiology. For these reasons, they tend to be noisier than wet electrodes. Dry electrodes can also suffer more from movement artefacts if they are not securely fastened.

An alternative approach is to dispense with the resistive contact and couple capacitively through an insulating layer [4]. With this method the signal fidelity no longer relies on skin resistance, however they can also suffer from movement artefacts and charge sensitivity. In most embodiments of dry and insulated electrodes an active electrode structure is used with high impedance amplification [4-5]. This minimizes the noise due to cabling and transmission of the signal. Electric Potential Sensor (EPS) is a high performance version of the insulated active sensor.

With specific reference to EEG signal acquisition, evidence exists that smaller, lighter sensors with a higher array density are required in order to reduce movement artefacts and to allow for redundancy [6]. A comprehensive review of wet, dry and insulating electrode technologies concludes that insulated active electrodes offer the most promising solution for future healthcare applications [1]. More recent work on dry electrodes has included a trial of a 6 sensor EEG system [7] and concludes that this could offer a cost effective solution for brain-computer interfacing. A clinical comparison of concurrent measurements with wet and dry EEG electrodes concludes that a high degree of correlation is seen and that dry electrodes offer better long-term performance [8]. New work on motion artefact reduction relies on the simultaneous measurement of the contact impedance of each sensor [9] using a small a.c. current (20 nA @ 1 kHz) and multiple dry spring loaded contacts in each sensor to introduce redundancy. Other workers have designed quasi-dry polymer electrodes which use a small quantity of moisturizing agent to address these problems [10].

In summary, EPS technology has already demonstrated that problems such as offset potentials, signal drift, ease of usability, and invasiveness can be addressed for electrocardiogram (ECG) data acquisition where the inherent DC stability and short settling time of the sensors differentiate them from other insulated electrode implementations [11]. However, the low frequency noise performance required for accurate EEG data acquisition is considerably more stringent and it is this important parameter which will be addressed in this paper. A review of sensor developments for healthcare [11] discusses the low frequency noise performance of a number of active sensors and characterizes them in

terms of the noise spectral density at 1 Hz. This is a useful indicator of the performance for EEG use and gives values ranging from $2 \mu\text{V}/\sqrt{\text{Hz}}$ to $10 \mu\text{V}/\sqrt{\text{Hz}}$, however these values will increase at lower frequencies due to $1/f$ noise.

The aim of the present paper is to examine whether the signal-to-noise performance of the EPS system is comparable to – or better than – that of a conventional electrode system, specifically in the 0.1-10 Hz bandwidth.

The design and specifications of the EPS sensor used in these experiments are described in Section 2, along with details of the commercial system used for comparing EPS with gel electrodes. In Section 3 the EPS results for free running (spontaneous) EEG are described, followed by data for two event-related potential (ERP) studies in Section 4. The second ERP experiment outlines a comparative study conducted between the two systems. Section 5 discusses three methods for quantifying noise of an EEG recording device, relevant to our EPS system.

2. Prototype Sensor and Systems

The prototype Sussex EPS device for this project is based on an auto-zero operational amplifier, chosen to give the lowest possible low frequency noise [12]. The absence of $1/f$ noise in these devices makes them ideal for use with signal frequencies ~ 10 Hz or less, with a quoted noise performance of $22 \text{ nV}/\sqrt{\text{Hz}}$ and $5 \text{ fA}/\sqrt{\text{Hz}}$. The input capacitance is $\sim 8 \text{ pF}$ with an associated voltage noise between 0.1-10 Hz of $0.5 \mu\text{Vp-p}$. After consideration of the expected signal amplitudes and frequency the sensor was configured to have an operational bandwidth of 0.1 Hz to 78 Hz and a voltage gain of $\times 50$. The voltage gain was distributed between two stages with $\times 5$ and $\times 10$ respectively for the first and second stages. The operation and circuit details of EPS devices have been published previously by the authors [13]. Here, the sensors are operated from split symmetric power supply rails of $\pm 2.5 \text{ V}$. Two versions were produced with different electrode sizes to enable reliable contact to be made to different parts of the body. The electrodes are electrically insulated through an anodized electrode with diameters of either 12 mm or 18 mm. In both cases the sensors were housed in inert stainless steel machined housings with the electronics fabricated in surface mount on a printed circuit board (PCB) compatible with epoxy potting compounds. Potted sensors are designed to be immersed in alcohol for sterilization purposes.

The gain and operational bandwidth of the sensors was confirmed using a standard spectrum analyzer to be as specified. The most significant parameter for the specification of the sensor in this particular application is the voltage noise referred to the input. This was measured by placing the sensor in a screened environment and recording the spectral noise density over a 1 kHz bandwidth. From this

data, shown in Fig. 1, two numbers are produced to characterize the noise performance: the spot noise figure at 1 Hz and the integrated noise from 0.1 Hz to 10 Hz. The results obtained for the voltage noise measurements are: $30 \text{ nV}/\sqrt{\text{Hz}}$ at 1 Hz and $0.2 \text{ } \mu\text{Vp-p}$

from 0.1 to 10 Hz; consistent with the data provided by the manufacturer. The absence of $1/f$ noise in this data confirms that the auto-zero amplifier used in this design is performing as expected.

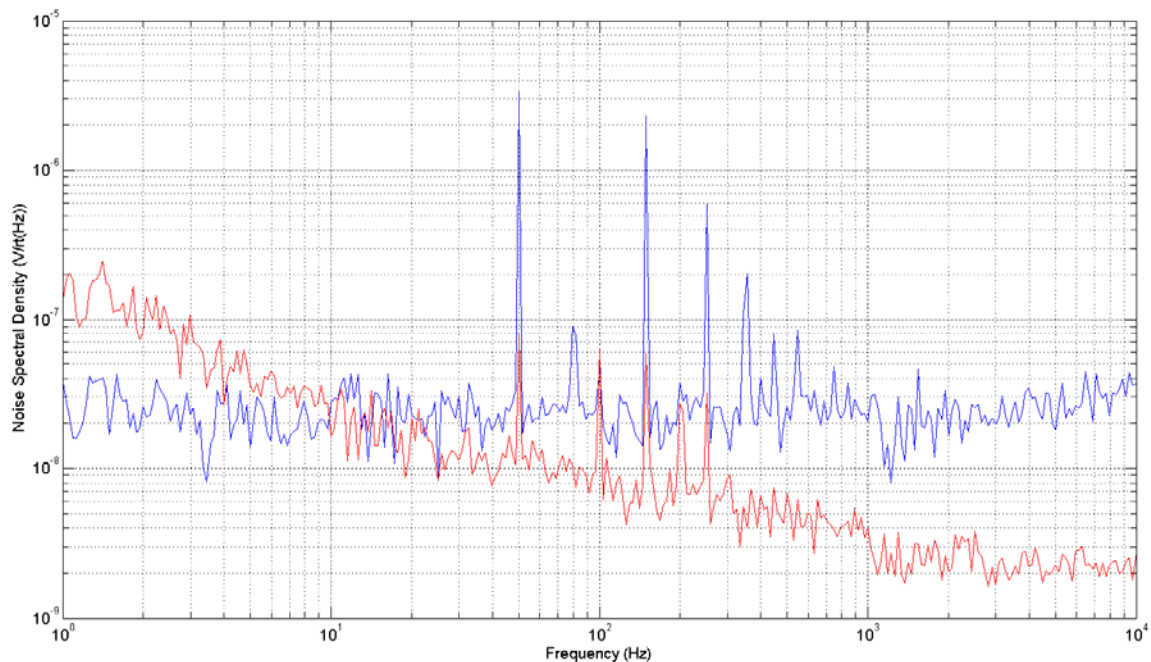


Fig. 1. Noise spectral density plot for prototype auto-zero sensor in comparison with a JFET input stage amplifier. The blue trace represents the prototype sensor. A lack of typical $1/f$ operational amplifier noise can be observed. Although the red trace has lower noise for frequencies higher than 20 Hz, the prototype sensor has lower noise in 1 to 10 Hz region (which is where the signal of interest lays). The voltage noise referred to input is measured as $30 \text{ nV}/\sqrt{\text{Hz}}$ at 1 Hz.

In order to confirm, at an early stage in the design process, that the sensor design was both suitable for high quality EEG signal acquisition and that it was compatible with commercial systems and practice we interfaced the sensors to a TMS International (TMSi) system currently in use in the School of Psychology at Sussex. This also enabled us to perform direct comparisons with wet gel electrode measurements. The prototype sensors were interfaced to a Refa8 amplifier produced by TMS International [14] with 64 EEG channels at 24 bit resolution with an input noise of $1 \text{ } \mu\text{V}_{\text{rms}}$. All electrode cables have active shielding to reduce 50 Hz mains interference and cable movement artefacts. In the comparative data presented here the TMS International acquisition system and data processing were applied to both sets of data.

In order to provide a comprehensive comparison between the Sussex EPS prototype and the commercial system two different types of EEG data were measured. First we recorded free running EEG focusing on the (well known) 'alpha blocking' signal.

The second type of EEG data recorded were event related potentials (ERPs). Two experiments were run to elicit ERPs: The first was a simple visual "oddball paradigm" [15], and the second a simple visual face perception [16].

In the case of both the EPS and commercial EEG systems, reference electrodes/sensors were placed on left and right mastoid positions. Other sensors/electrodes were placed at scalp positions dictated by the specific experimental paradigm, according to the International Standard 10-20 electrode location system [17]: left and right occipital (O1 and O2) for alpha-blocking; midline parietal (Pz) for the visual oddball paradigm; and left/right parietal (P7 and P8) for the face processing paradigm.

The recorded data from the paradigm-specific sensors/electrodes were offline re-referenced to linked mastoids, by averaging data from the two mastoid positions and subtracting it from each paradigm-specific sensor/electrode.

3. Spontaneous EEG

Initial measurements were carried out on the free running EEG to verify that the prototype sensor had an appropriate noise performance to allow EEG data to be seen. The alpha signal is observed when the eyes are closed and is characterized by an increase in amplitude of the 8-13 Hz EEG signal. Alpha activity can be recorded from 95 % of people [15] and is

blocked when the eyes are open. The signal may be seen in real time in the time domain, as shown in Fig. 2, where the alpha blocking caused by opening the eyes may be seen clearly.

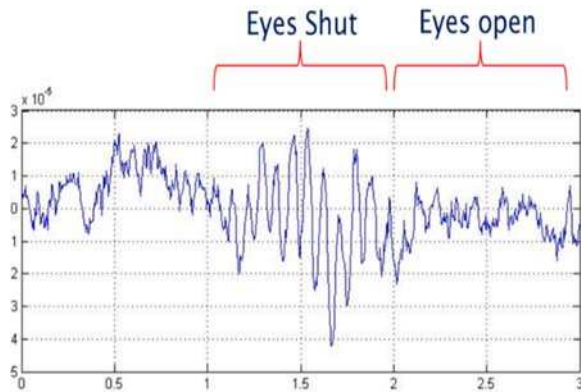


Fig. 2. Time domain data showing the alpha blocking phenomena measured using the prototype sensor.

Alternatively, if the time series data is Fourier transformed we see a broad peak in the frequency domain data. This is illustrated in Fig. 3 where a 40 s section of time series alpha data has been Fourier transformed to show a clear ~ 10 Hz peak.

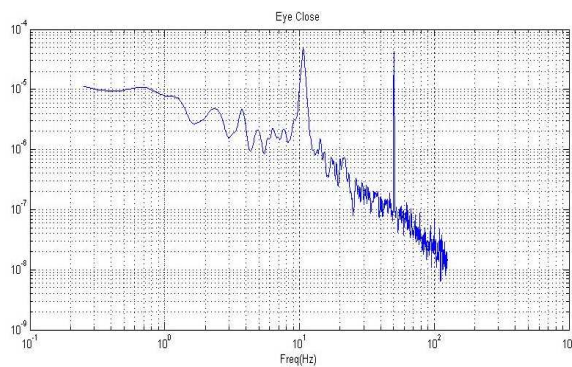


Fig. 3. Fourier transform of time domain data showing a broad alpha signal peak at ~ 10 Hz. The participant was asked to close their eyes for period of 40 s. The second peak is the 50 Hz mains signal.

A residual 50 Hz mains interference signal may also be seen (the rightmost peak in Fig. 3), however the common mode rejection ratio (CMRR) is sufficient to reduce this amplitude to be comparable to the measured signal.

4. Event Related Potentials

Event-related potentials (ERPs) are time-locked EEG responses to specific events, usually discrete sensory inputs. ERPs are characterized by deflections from baseline (baselines are typically computed over

the pre-stimulus period) at specific time-points post-stimulus. The 'oddball effect' is the ERP difference reflecting a contrast between expected and unexpected (frequent and infrequent) stimuli.

Two different stimuli are presented on a screen with one event randomly chosen to occur more often than the other. A volunteer is asked to press the space bar only when they are presented with one of the two events. Typically, signals are averaged and band-pass filtered at 0.1 to 30 Hz, again we have followed this standard practice. A typical oddball paradigm presents letters e.g. X and O on a monitor with 80 % and 20 % relative frequency respectively [15]. The letters are displayed for 100 ms with a blank screen presented for 1.4 s between each letter. In this experiment, the O is the 'oddball' stimulus.

Little information may be gained from real-time data in ERP paradigms, so that averaging over a number of events is usually needed [18]. The data is usually recorded using the Pz position and a reference electrode (s). Fig. 4 shows the results for 67 averages, 53 for the 'X' and 14 for the 'O'. There is a clear time-difference in the major ERP component between the 'X' and 'O' data as expected [19]. This experiment contained a relatively low number of trials for an ERP study, indicating that the EPS prototype sensor is highly capable in this challenging mode of operation.

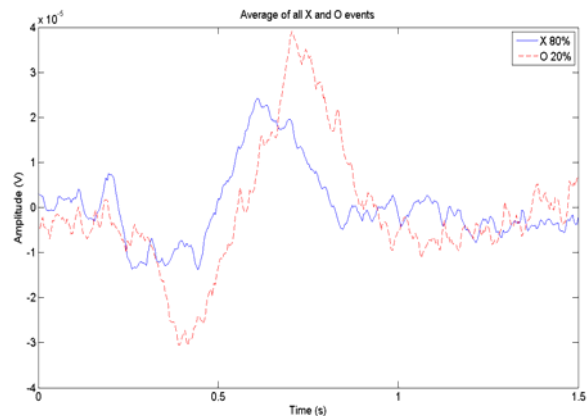


Fig. 4. Averaged ERP data, recorded from Pz, collected by the EPS, showing the oddball effect (delayed response to the rare stimulus).

In a second ERP study we looked at the sensitivity of the EPS for recording category specific effects in a standard face processing study. Three different images were presented to the subjects: faces, inverted faces and scrambled faces. The resulting ERP waveforms are displayed for the wet gel electrodes in Fig. 5 and the EPS in Fig. 6. For both sensor types measurement electrodes were located at the P7 and P8 positions, with the reference sensors on M1 and M2 (left and right mastoids).

In order to improve the quality of the data and to allow a more accurate comparison to be conducted a grand average was produced over 4 subjects.

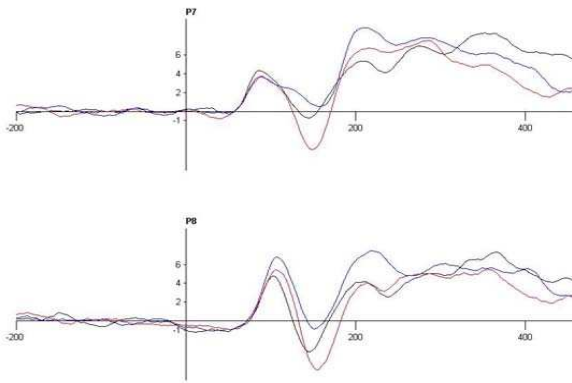


Fig. 5. Grand average of 4 participants ERP face data from wet gel electrodes, positions P7 and P8. Faces (black line); inverted faces (red line) and scrambled faces (blue line). Stimulus onset at 0 ms.

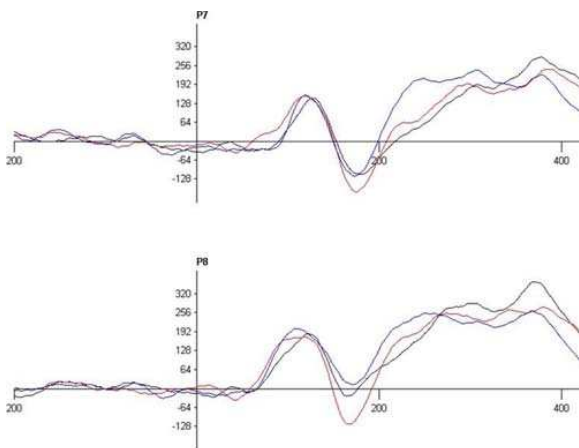


Fig. 6. Grand average of 4 participants ERP face data from EPS, positions P7 (top) and P8 (bottom). Faces (black line); inverted faces (red line) and scrambled faces (blue line). Stimulus onset at 0 ms.

Visual inspection of the results of these ERP measurements show that the grand averaged data for the EPS system is remarkably similar to that produced by a standard commercial EEG system, specifically in terms of demonstrating stimulus-category specific patterns of activity. Moreover, the apparent signal to noise ratio appears to be strictly comparable. From these initial results we therefore conclude that the current prototype EPS device has an adequate level of noise performance for all the EEG signals observed during these tests.

5. EEG Quality

Quantification of noise in an EEG recording is complex due to the signal processing that is applied to the recorded signals. However, if different aspects of an EEG signal are studied individually then useful information can be gained. Here three methods are used to separately characterize the low frequency drift, ERP noise, and broadband noise.

5.1. Raw Signal

EEG data is commonly preprocessed with high and low pass filters to remove any drift caused by wet gel electrodes (and other factors) and to reduce the effects of out-of-band noise. However if the raw signal is inspected for a long period of time then slow drift can be observed. These drifts are due to a combination of different effects such as variations in skin resistance [20] and alteration in half-cell potential of Ag/AgCl electrodes [3].

Fig. 7 displays 10 minutes of EEG recording from both the EPS and wet gel systems. Here the raw signal can be seen with a drift in the wet gel electrode of up to 2 mV. This is often compensated for by using high supply rails to avoid railing the signal, and high precision 24 bit digitizers to be able to record these small signals over larger ranges. This effect is not seen in the EPS as the sensor does not have a DC response.

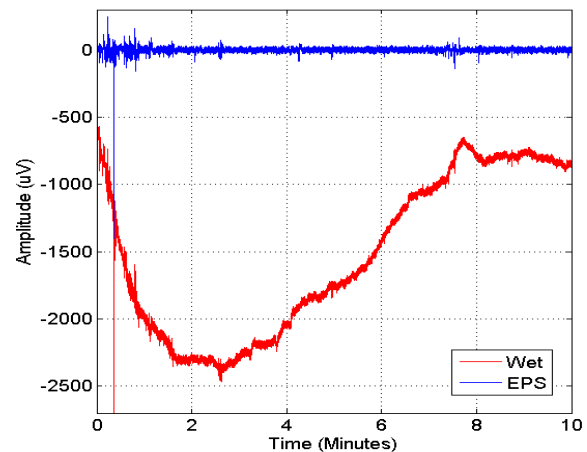


Fig. 7. The raw signal can be seen to drift with time when recorded with a wet gel electrode, this is not the case when compared with the EPS drift over a 10 minute recording.

5.2. Signal to Noise Ratio

As demonstrated in Section 3, when a person closes their eyes a ~ 10 Hz oscillation appears in their EEG. This power increase in this alpha band of EEG is reversed upon opening the eyes ('alpha blocking'). As Alpha is a signal superimposed on the background EEG and broadband noise, it is possible to define this evoked increase in the Alpha band power by comparing it to the background variations. Signal to noise ratio (SNR) can be calculated using the following equation [20].

$$SNR = 10 \log_{10} \frac{EEG(10Hz)^2}{\text{var}(EEG) - EEG(10Hz)^2} \quad (1)$$

A 30 second recording of an Alpha signal from a single participant was gathered simultaneously by the

prototype EPS and the TMSi system. This was formed by a differential recording of Oz-Fz. Using FFT, power of the alpha signal at 10 Hz was calculated across this data. The EPS had a SNR of -26.0244 dB compared to a value of -33.2565 dB for the wet gel electrode. This provides values smaller than zero due to the small amplitude of the Alpha signal compared with broadband noise and background EEG. Showing that for this recording the EPS displays a slightly better SNR than a standard EEG system.

5. 3. ERP Noise

Event related potentials are the most commonly studied signal type in EEG. Thus it is important to assess the SNR of an averaged ERP. Fig. 6 and Fig. 7 both present grand average ERPs from the face perception study. The pre-stimulus section (-200 ms to 0 s) of both figures shows no significant variations from the baseline. Assuming no stimulus-specific neuroelectrical activity prior to the trigger signal then any deviations can be associated with noise. The Root-mean-square (RMS) voltage of this time period presents a measure of noise activity independent of frequency [20]. The closer the RMS is to zero the less affected the ERP signal is to non-event related activity. Table 1 contains RMS noise values of 4 subjects who participated in the face perception study.

Table 1. ERP RMS Noise.

| Subject No. | Pre stimulus ERP RMS Voltage (μV) | |
|-------------|--|--------|
| | Wet | EPS |
| 1. | 1.0503 | 0.2574 |
| 2. | 0.8073 | 0.6030 |
| 3. | 0.8992 | 0.1642 |
| 4. | 0.2702 | 0.3711 |
| Mean | 0.7568 | 0.3489 |
| STD | 0.3395 | 0.1893 |

These RMS values show that the EPS displays a similar noise profile to standard wet electrodes. The variations in mean and SD was expected as these signals were not recorded simultaneously.

6. Conclusions

The Sussex EPS prototype has been verified as suitable for the acquisition of both free running EEG and ERPs. The prototype performance has also been

verified by interfacing with a commercial system, and by comparing results with those from wet gel electrodes. All results obtained indicate that the Sussex EPS prototype produces strictly comparable signal-to-noise ratios to conventional wet gel electrode devices for both free running and ERP measurements. The low frequency noise has been identified as the key performance indicator for capacitively coupled active sensors. In particular, the frequency range of typical EEG signals lies within the 1/f noise region of most active devices. The use of an auto-zero operational amplifier within the prototype sensor has been demonstrated to eliminate this problem and yield results which are strictly comparable to wet gel electrodes.

Acknowledgements


The work presented here forms part of the DeNeCoR project which is funded by the European ENIAC Joint Undertaking (JU) and the Technology Strategy Board (TSB). Special thanks to the Dr. Mortimer and Theresa Sackler Foundation, for supporting the Sackler Centre for Consciousness Science.

References

- [1]. A. Searle, L. Kirkup, A direct comparison of wet, dry and insulating bioelectric recording electrodes, *Physiological Measurement*, Vol. 21, 2000, pp. 271-283.
- [2]. D. Prutchi, M. Norris, Design and Development of Medical Electronic Instrumentation, *John Wiley and Sons*, New Jersey, 2005.
- [3]. Y. M. Chi, T.-P. Jung, G. Cauwenberghs, Dry-Contact and Noncontact Biopotential Electrodes: Methodological Review, *IEEE Reviews in Biomedical Engineering*, Vol. 3, 2010, pp. 106-119.
- [4]. A. J. Clippingdale, R. J. Prance, T. D. Clark, H. Prance, T. Spiller, Ultra-high impedance voltage probes and non-contact electrocardiography, in *Sensors VI: Technology, Systems and Applications*, K.T.V. Grattan (Ed.), *IOP Publishing*, 1991, pp. 469-472.
- [5]. E. Spinelli, M. Haberman, Insulating electrodes: a review on biopotential front ends for dielectric skin-electrode interfaces, *Physiological Measurement*, Vol. 31, 2010, pp. S183-S198.
- [6]. B. A. Tahari, R. T. Knight, R. L. Smith, A dry electrode for EEG recording, *Electroencephalography and Clinical Neurophysiology*, Vol. 90, 1994, pp. 376-383.
- [7]. F. Popescu, S. Fazli, Y. Badower, B. Blankertz, K. R. Muller, Single Trial Classification of Motor Imagination Using 6 Dry EEG Electrodes, *PLoS ONE*, Vol. 2, Issue 7, July 2007, pp. e637.
- [8]. G. Gargiulo, *et al.*, A new EEG recording system for passive dry electrodes, *Clinical Neurophysiology*, Vol. 121, 2010, pp. 686-693.
- [9]. A. Bertrand, V. Mihajlovic, B. Grundlehner, C. van Hoof, M. Moonen, Motion artifact reduction in EEG recordings using multi-channel contact impedance

- measurements, *Biomedical Circuits and Systems Conference (BioCAS), IEEE*, Oct. 2013, pp. 258-261.
- [10]. A. R. Mota, *et al.*, Development of a quasi-dry electrode for EEG recording, *Sensors and Actuators*, Vol. 199, 2013, pp. 310-317.
- [11]. H. Prance, Sensor Developments for Electrophysiological Monitoring in Healthcare, in Applied Biomedical Engineering, Dr. Gaetano Gargiulo (Ed.), *InTech*, 2011, Available from: <http://www.intechopen.com/books/applied-biomedical-engineering/sensor-developments-for-electrophysiological-monitoring-in-healthcare>, [retrieved: June, 2014]
- [12]. AD8628 datasheet, *Analog Devices, Inc., One Technology Way*, P.O. Box 9106, Norwood, MA 02062-9106, U.S.A., [retrieved: June, 2014], Available from: http://www.analog.com/static/imported-files/data_sheets/AD8628_8629_8630.pdf
- [13]. C. J. Harland, T. D. Clark, R. J. Prance, Electric potential probes - new directions in the remote sensing of the human body, *Measurement Science and Technology*, Vol. 13, 2002, pp. 163-169.
- [14]. Refa8 amplifier datasheet, *TMS International*, Zutphenstraat 57, 7575 EJ Oldenzaal, The Netherlands, Available at: <http://www.tmsi.com/products/systems/item/refa>, [retrieved: June, 2014]
- [15]. P. L. Nunez, R. Srinivasen, Electric Fields of the Brain, in *The Neurophysics of EEG*, 2nd Edition, *Oxford University Press*, 2005.
- [16]. A. J. Calder, *The Oxford handbook of face perception*, *Oxford University Press*, Oxford, 2011.
- [17]. M. Fatoorechi, *et al.*, Comparison of Dry and Wet Electrode Systems for Spontaneous and Event Related Electroencephalograms, in *Proceedings of the 5th International Conference on Sensor Device Technologies and Applications (SENSORDEVICES'14) 16-20 November 2014*, Lisbon, Portugal, pp.71-74.
- [18]. J. Malmivuo, R. Plonsey, *Bioelectromagnetism: Principles and Applications of Bioelectric and Biomagnetic Fields*, *Oxford University Press*, 1995.
- [19]. Steven J. Luck, *An introduction to the event-related potential technique*, *MIT Press*, 2014.
- [20]. Kappenman Emily S., Steven J. Luck., The effects of electrode impedance on data quality and statistical significance in ERP recordings, *Psychophysiology*, 47, 5, 2010, pp. 888-904.
- [21]. Y. M. Chi, Yu-Te Wang, Yijun Wang, Maier C., Tzyy-Ping Jung, Cauwenberghs G., Dry and Noncontact EEG Sensors for Mobile Brain-Computer Interfaces, *IEEE Transactions on Neural Systems and Rehabilitation Engineering*, Vol. 20, No. 2, March 2012, pp. 228-235.

2015 Copyright ©, International Frequency Sensor Association (IFSA) Publishing, S. L. All rights reserved. (<http://www.sensorsportal.com>)



Handbook of Laboratory Measurements and Instrumentation

Maria Teresa Restivo
Fernando Gomes de Almeida
Maria de Fátima Chouzal
Joaquim Gabriel Mendes
António Mendes Lopes

The Handbook of Laboratory Measurements and Instrumentation presents experimental and laboratory activities with an approach as close as possible to reality, even offering remote access to experiments, providing to the reader an excellent tool for learning laboratory techniques and methodologies. Book includes dozens videos, animations and simulations following each of chapters. It makes the title very valued and different from existing books on measurements and instrumentation.

IFSA
International Frequency Sensor Association Publishing

Order online:
http://www.sensorsportal.com/HTML/BOOKSTORE/Handbook_of_Measurements.htm